ArtUs EXT-1H ArtUs EXT-2H

Ultrasound Diagnostic System



USER GUIDE

Manufactured by

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1. INTRODUCTION



<u>CAUTION</u>: United States federal law restricts this device to be used by, or on the order of, a licensed physician.

Dear customer,

ArtUs EXT-1H/2H system is intended for multipurpose ultrasound examinations, based on electronic linear and convex scanning.

It is an ideal budget solution for hospitals, specialized diagnostic centers, public and private clinics.

Here in the **User Guide** you can find information about **ArtUs EXT-1H/2H** and its safety and maintenance information.

Echo Wave II Software Operation Manual contains a description of the controls.

1.1. About the system / Intended use

ArtUs EXT-1H/2H system is intended to be used for applications in fetal, abdominal, pediatric, small organ (breast, thyroid, testicles), adult cephalic, musculo-skeletal (conventional), musculo-skeletal (superficial) cardiac adult, cardiac pediatric, peripheral vessel (B and M-mode, combined modes imaging, including imaging for needle guidance) It is possible to provide diagnostic information outside of an imaging lab, including at the bedside systems, for navigated medical applications and in operating rooms/critical care units.

ArtUs EXT-1H/2H ultrasound systems provide many different scanning technologies: B, B+B, 4B, B+M, M, CFM, Tissue Harmonic Imaging (THI). Echo images can be either full size or zoomed.

Unlike ordinary ultrasound devices, this scanner is based on modern digital technologies. PC application enables many powerful innovative features such as:

- user friendly, easy-to-use intuitive graphic user interface
- echo image storage on hard disk or other devices
- storage of a sequence of full-size echo images (cine) with the possibility to save it in video file format
- image and cine file formats enable using other applications for viewing stored data
- using a variety of peripheral devices
- image and video sending by E-mail.

A variety of available ultrasound transducers provides many different applications for examinations in therapy, obstetrics, gynecology, urology, pediatrics, oncology and other areas.

Common view of ArtUs EXT-1H is shown below (without transducer).



Common view of ArtUs EXT-1H is shown below (without transducer).



1.2. Delivery set

Beamformer	•	
Operation Manual	•	
This User Guide	•	
Software and manuals (eIFU)	•	
USB cable	•	
Power supply (medical grade)	•	
Ultrasound transducer(s)	Types and quantity	
	defined by customer	

1.3. About the system software

Your diagnostic system contains **Echo Wave II** software to control its operation. TELEMED provides the latest **Echo Wave II** software version and drivers package together with your system. In the software the unique technologies making the intellectual property of TELEMED company are used. Latest software versions can be downloaded directly on the Internet from http://www.telemed.lt.

1.4. Technical Specifications

 Table 1 contains technical specifications of ArtUs EXT-1H/2H.

Table 1

IMAGIN	G MODES
1.	В
2.	B+B
3.	4B
4.	B+M
5.	Μ
6.	B-steer for linear transducers
7.	Compound for linear and convex transducers
8.	Virtual convex for linear transducers
9.	Expanded view angle for convex transducers
10.	Color Doppler (CFM)
11.	Power Doppler (PDI)
12.	Directional Power Doppler (DPDI)
13.	Pulsed Wave Doppler (PWD)
14.	B+PWD (Duplex)
15.	Inverted Tissue Harmonic Imaging (ITHI)
16.	Tissue Harmonic Imaging (THI)
17.	Parallel beam forming
18.	RF data access using SDK library
ULTRAS	SOUND IMAGING
1.	ultrasound image size: automatically adjustable to screen resolution
2.	gray scale: 256
3.	color scale: 256
4.	full motion and full-size real-time ultrasound imaging, up to 120 fps (depends on
	selected scanning depth, angle, focusing mode, Lines Density setting, computer
_	speed)
5.	cine recording/play: several thousand frames (depends on computer memory
-	size and scanning mode)
6.	zoom mode: from 60% to 600% in all modes (Scan, Freeze, B, B+B, 4B, Doppler
_	modes, M-zoom, cine, etc.)

- 7. variable view area for maximizing frame rate: 6 steps
- 8. "FREEZE" mode

SCANNING METHOD

- 1. Electronic linear
- 2. Electronic convex
- 3. Electronic micro-convex

COLOR DOPPLER

- 1. PRF variable: 0.5-10 kHz
- 2. Wall filter settings: 3 steps (5%, %10%, 15% PRF)
- 3. Gain control: 40 dB
- 4. Angle steering for linear transducers: ±25°

- 5. Real-time spatial filter: 4 values
- 6. CFM palette: 10 maps
- 7. B/Color priority control
- 8. Color threshold control
- 9. CFM baseline control
- 10. Doppler frequency selection: 2-3 frequencies for each transducer
- 11. Color frame averaging: 8 values

DEPTH SELECTION

1. 2 – 30 cm (depth range depends on transducer type)

TRANSDUCERS

- 1. Ranging from 1.5 MHz to 18 MHz
- 2. Multi-frequency
- 3. Automatic transducer recognition

FOCUSING

- 4. Transmit: variable, 8 zones
- 5. Receive: point to point, dynamic

SIGNAL PROCESSING

- 1. Lines density control for better resolution
- 2. TGC control
- 3. Dynamic range
- 4. Overall gain control
- 5. M mode sweep speed control
- 6. Acoustic power control
- 7. Variable frame averaging
- 8. Brightness, contrast
- 9. Advanced gamma control: 8 fixed curves, 8 user defined (custom)
- 10. Scan direction, rotation, up-down controls
- 11. Negative / positive control
- 12. Bi-linear interpolation
- 13. Echo enhancement control
- 14. Noise rejection function
- 15. Speckle reduction function

FUNCTIONS

General Measurements and Calculations	 Mouse / trackball / keyboard operation of multiple calipers B-mode: Distance / Length / Area / Circumference / Volume / Angle / Stenosis % / A/B Ratio M-mode: Distance / Time / Velocity / Heart Rate / Stenosis % / A/B Ratio
--	---

Human Measurements and Calculation Packages	 General calculations package Obstetrics / Gynecology (OB / GYN) calculations package Gynecology (GYN) Abdominal exam measurements and calculations Urology Endocrinology Vascular exam measurements and calculations Cardiology
User Interface	 The set of predefined skin schemes for user interface User-friendly pop-up menus and dialog boxes Unlimited programmable presets for clinically specific imaging Image comment / save / recall browsing Anatomical icons with transducer position indicator
Image and video save / load	• JPG BMP PNG TIF AVI DCM DCM-JPG TVD TPD
Cine	 Recording up to 2048 frames to memory Play / Pause / Stop / Frame selection Saving ultrasound video file to disk Loading ultrasound video file from disk
Printing	System printer
Internet	 Direct E-mail sending function with image or video attachment
TV output	 Standard TV output using computer's display adapter (option)
ULTRASOUND SOFTWA	RE
Drivers	TELEMED Drivers Package
Software	• Echo Wave II software (B/W + Doppler modes)
DIMENSIONS AND WEIG	НТ
Dimensions W x D x H, mm	136 x 189 x 28 (ArtUs EXT-1H) 140 x 205 x 65 (ArtUs EXT-2H)
Weight, kg	0.66 (ArtUs EXT-1H) 1.10 (ArtUs EXT-2H)
POWER CONSUMPTION	
12 VDC, 3.5 A Max	 External AC medical grade power supply (100-240 VAC, 50- 60 Hz), Class II, XP Power AKM65US12C2

5 VDC, 0.13 A Max	USB 3.0 connection	
SAFETY		
Electromechanical safety	 IEC 60601-1 Medical electrical equipment part 1: General requirements for safety. Class II Type BF applied part 	
EMC/EMI standards	 European Norm EN 55011:1998 (CISPR 11:1999) Industrial, scientific and medical (ISM) radio-frequency equipment. Radio disturbance characteristics. Limits and methods of measurement 	
Ultrasound exposure	 CEI/IEC 61157:1992, International Electrotechnical Commission, Requirements for The Declaration of the Acoustic Output of Medical Diagnostic Ultrasonic Equipment AIUM/NEMA: Standard for real-time display of thermal and mechanical acoustic output indices on diagnostic ultrasound equipment.1992 	
Degree of protection (watertight)	 Main unit IPX0 Transducers IPX7 (only the area of the transducer array acoustic window) 	
OPERATIONAL ENVIRO	NMENT	
Nominal operational environment	 Environment temperature: 10 - 40 ° C Relative humidity not to exceed: 85 % Atmospheric pressure: 70 - 106 kPa 	

2. <u>SAFETY</u>



CAUTION:

Please read this information before using the diagnostic system. It applies to the ultrasound system, transducers, accessories and peripherals.



WARNING:

In the event of detecting a discrepancy regarding patient safety requirements (occurrence or probability of risk) you must to inform the local dealer and the manufacturer immediately.

2.1. Electrical safety

This system complies with the applicable medical equipment requirements and meets IEC 60601-1, Class I Type BF safety requirements.

NOTE:

All persons connecting computer equipment as medical appliance are configuring a medical system and are therefore responsible for ensuring that the system complies with IEC 60601-1. The achievement of PC compliance with the IEC 60601-1 requirements is based on electrical safety. A standard PC power supply is almost certain to not comply with IEC 60601-1 electrical requirements in several ways, e.g. leakage current requirements, dielectric strength requirements.



One possible solution is powering the PC (and computer monitor) via a 1:1 medical insulation transformer, which has been designed to meet IEC 60601-1 requirements. The best solution is a fully IEC 60601-1 certified PC or a battery-operated portable PC and wireless peripheral devices.

All systems (including monitors and other connected parts) must be configured to comply with IEC 60601-1. If in any doubt please contact the technical service department of your local representative.

Note that regardless of the above stipulations all personal computers used should be approved regarding the IT (information technology) safety standards for electrical equipment (such as IEC 60950 or equivalent).

The electrical specification is shown below and is labeled on the rear panel of a scanner.

To avoid electrical shock only use the supplied cables and connect it to properly earthed power socket. Do not use a three pin - two pin adapter. This defeats the whole purpose of earthing for safety reasons. Systems should be operated within the voltage limits.

If the ultrasound scanner will be moved or left unused for a long period of time without being switched on it is recommended to disconnect it from a power supply.

If a scanner is to be switched on, do not interrupt this while operating the system and while the ultrasound software is being loaded. The time for this operation is approximately 1 minute.

To avoid the risk of electrical shock and fire hazard:

- before using the transducer, inspect the transducer face, housing, and cable and do not use the transducer if the transducer or the cable is damaged;
- always disconnect the AC power supply from the system before cleaning the system;
- do not use any transducer that has been immersed beyond the specified cleaning or disinfection level;
- inspect the power supply, AC power supply cable and electrical plug on a regular basis to ensure they are not damaged;
- do not supply power to the system from unapproved AC power supply, not supplied by TELEMED;
- only use accessories and peripherals recommended by TELEMED.

WARNING:

To allow quick and easy disconnecting of equipment from power source in case of emergency place the equipment so that there is a gap at least 10 cm between the rear panel and the other object (wall, toher equipment, tec.) and the power plug is accessible by hand.

WARNING:

To avoid the risk of electrical shock do not open the cover of device. There are no parts that you can repair yourself. In case of difficulties please contact the TELEMED service department or your nearest local authorized distributor.

2.2. Equipment protection

To protect your ultrasound system, transducer and accessories, please follow these precautions:

- excessive bending or twisting of electrical cables can cause a failure or intermittent operation;
- incorrect cleaning or disinfecting of any system part can cause permanent damage, for cleaning and disinfecting instructions see the relevant chapter below;
- do not use solvents such as thinners/benzene or abrasive cleaners on any parts of the system;
- do not spill liquids on the system;
- incorrect assembly or configuration and using an incorrect power source may damage the system.



WARNING:

Ultrasound transducers can easily be damaged by incorrect handling! Failure to follow these precautions can result in serious injury and equipment damage!

2.3. Biological safety



<u>WARNING:</u> Some transducer covers may contain talc and natural rubber latex. Examine the package labeling to confirm latex content. We strongly recommend that health-care professionals identify their latexsensitive patients, and refer to the FDA's March 29, 1991 Medical Alert on Latex products. Be prepared to treat allergic reactions promptly. NOTE: TELEMED diagnostic ultrasound systems and transducers do not

<u>NOTE:</u> TELEMED diagnostic ultrasound systems and transducers do not contain natural rubber latex that contacts humans.

Observe the following precautions related to biological safety:

- do not use the system if it displays erratic or inconsistent behavior;
- interruptions to the scanning sequence are signs of hardware failure that must be corrected before use;
- do not use the system if it displays artifacts on the LCD screen, either within the clinical image or on the area outside it;
- artifacts are indications of hardware and/or software errors that must be corrected before use;
- perform ultrasound procedures prudently, use the ALARA (As low As Reasonably Achievable) principle (see <u>APPENDIX</u>: Guidelines for the safe use of diagnostic ultrasound);
- devices are contraindicated for ophthalmic use or any application that causes the acoustic beam to pass through the eye.



WARNING:

At detection of discrepancy to patient's safety requirements (occurrence or probability of risk) you need to inform immediately the local dealer and the manufacturer.

2.4. Ultrasound exposure and ALARA principle

Perform ultrasound procedures prudently, use the ALARA (As low As Reasonably Achievable) principle (see <u>APPENDIX</u>: Guidelines for the safe use of diagnostic ultrasound).

The interactive system features or user controls that may affect the acoustic output are:

- acoustic output control,
- transmit frequency;
- scanning depth;
- transmit focal length;
- scanning angle.

Acoustic output also depends on the imaging mode selected. The choice of mode (B-Mode, M-Mode, B+M-Mode) determines whether the ultrasound beam is stationary or in motion. B+M-Mode has the highest acoustic output.

The default output level is factory calibrated and is based on device settings that yield an optimum image for the type of patient examination and do not exceed the following FDA recommended limits. This default level is set:

- when the system is first turned on;
- when the transducer is first turned on.

It is highly recommended to set the default level:

- when changing from one exam category to another;
- when changing from one application to another;
- when changing from one transducer to another;
- when a new patient is entered.

Once an optimal image is achieved, the need for increasing acoustic output or prolonging the exposure cannot be justified. Watch the POWER level (on-screen display) permanently. Whenever possible, controls and system features should be used to optimize the image before increasing the acoustic output level. Follow the ALARA principle during all patient examinations.

The **ArtUs** devices employ the ALARA principle in configuring factory defaults.



CONTRAINDICATION:

This device is contraindicated for ophthalmic use or any application that causes the acoustic beam to pass through the eye.

Ultrasound waves used in diagnostic system have frequencies ranging from 2 MHz to 18 MHz Sound waves with such frequencies are weakened in the air, so can be measured, for example, in water. Ultrasound waves sent by a converter are so weak (medium intensity less than 100 mW/cm²), that, according to International Electrotechnical Commission (IEC 1157) standards (well within AIUM/NEMA standards), they do not have any impact on patient health (however any unnecessary exposure should be avoided).

Detailed information is found in <u>APPENDIX</u>: Guidelines for the safe use of diagnostic ultrasound.

2.5. Cybersecurity

Vulnerabilities in cybersecurity may represent a risk to the safe and effective operation of networked medical devices. Store only relevant and necessary software on working computers.

Network administrators in healthcare organizations and information technology providers should assure an adequate degree of protection from threats such as viruses and worms to avoid the risk of any unauthorized access to the network or the medical device/database. Please share with your local administrator detailed settings information from this document section **"Windows configuring"**.

2.5.1. Information Security

When entering and saving data it is your responsibility to protect your security credentials and the personal information of patients.

2.5.2. Network Security

Use a network supporting Wi-Fi 802.11n and WPA (Wi-Fi Protected Access) or WPA2 (Wi-Fi Protected Access II) as your security protocol.

Refer to your network equipment documentation for setting wireless network security.

Do not use untrusted wireless access points, it may allow third party to perform harmful actions. When no secure access point is available, operate in Wi-Fi Direct mode – it will automatically set up encryption.

For security purposes:

• Use secure passwords

• Use secure protocols, secure wireless equipment with the latest firmware/software

• Lock your PC

The following actions could introduce new risks to patients, operators and third parties:

- Changing network configuration
- Connecting to additional networks or disconnecting from existing networks
- Upgrading to new equipment or updating existing equipment

2.5.3. Confidentiality

If you want the data encrypted, connect to a:

- Wi-Fi network where only trusted parties are permitted. The Wi-Fi network encrypts all image data sent from other Wi-Fi networks.
- Wi-Fi Direct network. The Wi-Fi Direct network encrypts all image data, and because no other users are on the Wi-Fi Direct network, the image data is confidential. Because Wi-Fi Direct network is a peer-to-peer connection using the Wi-Fi protocol, it disallows other users from connecting, thereby reducing DDOS (Distributed Denial of Service) attacks.

2.5.4. Integrity

Integrity of the data transmitted between the device and network is assured as follows:

- Authenticated encryption prevents malicious users from intercepting and modifying data.
- TCP channels used over Wi-Fi ensures that data is delivered correctly.

2.5.5. Accountability

Ownership (i.e. the active user) of a PC is assigned to one user at a time. Once you begin using the PC, no other user can connect to the same device. All data transmitted between the device and network is owned by the active user.

2.6. Measurement Accuracy

WARNING:



Clinical diagnostic errors may result from the incorrect use of calculations. Review the referenced source of the stated formula or method to become familiar with the intended uses and possible limitations of the calculations. Calculation formulas and databases are provided as a tool to assist the user and should not be considered as an undisputed database when making a clinical diagnosis.

The accuracy of measurements is determined not only by the TELEMED Echo Wave II software but also by the proper use of medical protocols.

Distance and area/circumference measurements are displayed to 0.1 mm.

The following general assumptions can be made about the accuracy of any ultrasound system:

- Velocity of sound is constant 1540 m/s
- Velocity of sound uncertainty is 5%
- Caliper placement accuracy is one pixel (operator dependent)
- Measurement accuracy is based on the root-mean-square combination of all independent sources of error
- RMS errors are due to velocity of sound uncertainty, pixel error, and typical transducer geometry

Note: The below measurement accuracies apply to all transducers and to all modes.

The linear distance measurement components have the accuracy and range shown in the following tables:

2D Measure Accuracy and Range	System Tolerance	Accuracy By	Test Method	Range
Axial Distance	< ±2% or 1mm	Acquisition	Phantom**	0.1-20 cm
Lateral Distance	< ±2% or 1mm	Acquisition	Phantom**	0.1-20 cm
Diagonal Distance	< ±2% or 1mm	Acquisition	Phantom**	0.1-20 cm
Area ***	< ±4% plus 1% of full	Acquisition	Phantom**	0.1-1000
Trace & Ellipse	scale*			Cm ²
Circumference	< ±3% plus 1% of full scale*	Acquisition	Phantom**	0.1-70 cm
Angle	< ±5%	Acquisition	Phantom**	0 -180°

2D Measurement Accuracy

* Full scale for distance implies the maximum depth of the image.

** An ATS model 539 phantom with 0.7 dB/cm-MHz attenuation was used.

*** The area accuracy is defined using the following equation: % tolerance = $((1 + 1)^* (1 + 1$

**** The circumference accuracy is defined as the greater of the lateral or axial accuracy and by the following equation: % tolerance = ((maximum of 2 errors) * 100) + 0.5%.

***** To take into account which of the tolerances is greater.

M-mode Measurement and Calculation Accuracy

M-mode Measurement Accuracy and Range	System Tolerance	Accuracy By	Test Method	Range
Distance	< ±5% or 1mm	Acquisition	Phantom **	0.1-20 cm
Time	< ±2% plus 1% of full scale *	Acquisition	Phantom****	0.1-10 sec
Heart Rate	< +/- 2% + (Full Scale *** x Heart Rate/100) %	Acquisition	Phantom****	20-300 bpm

* Full scale for distance implies the maximum depth of the image.
** An ATS model 539 phantom with 0.7 dB/cm-MHz attenuation was used.
*** Full scale for time implies the total time displayed on the scrolling graphic image.

**** TELEMED special test equipment was used.

Other Measurement and Calculation Accuracy

Parameter		System Tolerance	Reference / Formula
Volume		< ±9%	4.2.3 Perimeter, square and volume measurements by Ellipse method
Fetus Weight	1 method	< ±16%	4.5.1 Hadlock85 (USA)
	2 method	< ±12%	4.5.2 Shepard82 (EU)
	3 method	< ±17%	4.5.3 Tokyo
	4 method	< ±16%	4.5.4 Osaka
Left Ventricle Volume	1 method	< ±15%	4.6.2 Cubed
	2 method	< ±11%	4.6.2 Pombo
	3 method	< ±13%	4.6.2 Teichholz
Stroke Volume		< ±15%	4.6.3 Stroke Volume
Ejection Fraction		< ±12%	4.6.4 Ejection Fraction
Cardiac Output		< ±15%	4.6.5 Cardiac Output
Left Ventricle Internal D	imension	< ±10%	4.6.6 Left Ventricle Internal
Fractional Shortening			Dimension Fractional
			Shortening
Aortic Valve Measurem	ents and	< ±8%	4.6.7 Aortic Valve
Calculations			Measurements and
			Calculations

3. LABELING

Table 2 describes the purpose and location of safety labels and other important information provided on the equipment.

Та	bl	е	2
	~ .	•	_

LABEL/SYMBOL	DESCRIPTION	LOCATION
CE	CE mark This mark is a declaration by the manufacturer that the respective component complies with the relevant directives and standards as issued by the European Union.	Rear panel (rating plate label)
Ŕ	Type BF Equipment (man symbol) IEC 878- 02-03 indicates BF type equipment which provides a particular degree of protection against electric shocks, particularly regarding allowable LEAKAGE CURRENT and reliability of the PROTECTIVE EARTH CONNECTION if present.	External (transducer outlet)
Â	Caution, consult accompanying documents This symbol advises the reader to consult the accompanying documents for important safety- related information such as warnings and precautions that cannot, for a variety of reasons, be presented on the device itself	Rear panel (along with rating plate label)
i	Consult instructions for use This symbol advises the reader to consult the operating instructions for information needed for the proper use of the device	Rear panel (along with rating plate label)
X	The symbol indicating separate collection for electrical and electronic equipment (Annex IV of Directive 2002/96/EC)	Rear/bottom panel
$\bullet \overleftarrow{\bullet} \bullet$	USB connector	Rear panel
	DC power input	Rear panel
	Manufacturer name and address	ID Label
REF	Model / Catalogue number	ID Label
\sim	Date of manufacture YEAR -MONTH- DAY	ID Label
IPX7	Protection (watertight, only the area of the transducer acoustic window)	Transducer
(01)04772057000116 (21)3971-170615-0143	UDI GS1 Data Matrix 2D barcode	ID Label Transducer

4. SYSTEM OVERVIEW

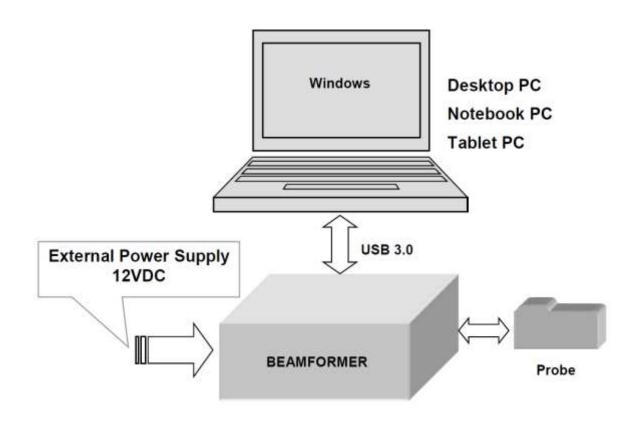
The **ArtUs EXT-1H/2H** system handles the multi-element transducers. Here is main information about Ultrasound Scanner. The system consists of, see figure below:

- Beamformer
- Power Supply +12VDC
- Ultrasound Transducer
- Windows PC (Desktop / Notebook / Tablet PC) with integrated USB 3.0 port



Attention:

ArtUs system requires Windows PC with integrated USB 3.0 or better port. For more technical details please refer to 5.2 paragraph.



4.1. Principle of operation

The ultrasound diagnostic system is based on the effect of ultrasound wave reflection from the tissue edges with different acoustic impedance levels. Ultrasound waves sent out by the transducer head are emitted into the patient's body. Reflections from the specific types of tissue and their external surface/edges cause partial reflections of the propagating sound wave. The return echo comes back to the transducer head and after being detected and amplified is displayed on the monitor screen as a pixel combination with various shades of brightness creating an ultrasound image.

4.2. Components & Modifications

4.2.1. Basic unit / Beamformer

Basic unit functions are:

- excite electric pulses to fire the transducer;
- ultrasound echo signals pre-amplification;
- compensation of the ultrasound attenuation due to travel depth;
- re-ordering the receiving signal sequence and focusing by applying the appropriate time delays;
- shifting the center frequency of BPF (band pass filter) to follow the frequency shift that occurs according to the travel depth;
- the ultrasound signal compression by means of Log Amplifier, detection of the echo signal envelope

4.2.2. Transducer Unit

The transducer unit is a piezoelectric transformer which provides the acoustical pulse used to examine the medium and is used for both transmission and reception (the transducer is used in pulse-echo mode). A voltage waveform is applied to the transducer and then converted into an acoustic waveform (inverse piezoelectric effect). An acoustic pulse is then partially transmitted and partially reflected by the intervening soft tissues structures in the body. The reflected acoustic waveform is received by the same transducer and is converted into a voltage waveform (direct piezoelectric effect). The transducer unit consists of many piezoelectric elements. The transducer enclosure has a relief to affix the scanning direction.

Transducer Type Order Code	System Frequencies, MHz	Radius / Length, mm	Abdominal	Cardiac	Obstetric	Pediatric	Small Parts	Transrectal	Transvaginal	Vascular	Veterinary
C5-2H60-A5	2-5	60	•		•	•					•
L12-5N40-A4	5-12	40				•	•			•	•
L15-7H40-A5	7-15	40				•	•			•	•
L18-7H30-A5	7-18	30				•	•			•	•
LF9-5N60-A3	5-9	60					•			•	•
LF11-5H60-A3	5-11	60					•			•	•
MCV9-5N10-A3	5-9	10						•	•		
P5-1S15-A6	1-5	-	•	•							•

4.3. Peripherals/Compatibility

ArtUs EXT-1H/2H scanner can work / operate with standard PC features:

- mouse
- keyboard

Optional accessories:

- Image Processing Packages
 - 3DView
 - PanoView
- Additional Transducers
- Transducers Carrying Cases

- SVGA monitor
- Laser printer 600 dpi, (preferred HP printers), optional
 - Biopsy Clip Bracket C- type (for convex transducers)
 - Biopsy Clip Bracket HL- type (for linear transducers)
 - PV-Biopsy Clip Bracket PV- type (for microconvex transducers)

5. USING THE SYSTEM

5.1. INSTALLATION WARNINGS

- The ultrasound scanner should be installed in a room specifically designated for this use, such as an ultrasound scanner laboratory, with an area of at least 10 m² and with window coverings to provide some ambient lighting.
- Power cords and other accessories used with the device must be supplied by the manufacturer or be of the same type as specified.
- To work correctly and ensure excellent results please use the complete set as recommended by the manufacturer.
- Do not connect too many electrical devices to the same power source. It may cause problems with operation of the device or even lead to the failure of the device.
- The device is still powered up when connected to a power source even if switched off.
- Any changes made to the ultrasound scanner by users are prohibited and may result in the guarantee no longer being valid.
- Always disconnect the scanner from the power supply in the event of:
 - Failure of the power supply cable;
 - Device being dropped;
 - Device fails to work correctly;
 - Strange noises or smoke coming from inside the device.
- Equipment damage due to improper use may void the warranty.
- Do not expose the device to excessive temperatures.
- When moving the scanner from a cold to a warm place please wait for 0,5 to 1 hour before switching on the device. This is necessary because of water condensation which may form on electronic parts.
- Do not use the scanner close to any moisture source or in place with high humidity.
- Do not use compressed air or vacuum cleaners when cleaning the device.
- Do not drop, hit or shake the device.
- Take care when working with ultrasound transducers. Transducers should be cleaned after work removing any gel and other deposits. Do not use any aggressive chemicals. To increase the lifespan of transducers always leave them after work with freeze acquisition.
- Transducer changing should only be done during FREEZE mode or POWER OFF mode.
- Ultrasonic waves have a low level of transmission in air and gases inside the living body. If air is present between the transducer and the skin the examination may be impossible to perform.
 - It is therefore necessary to apply an acoustic coupler (special gel, olive oil, liquid paraffin, etc.) so that the transducer sticks to the skin.
 - It is also impossible to examine regions of the body which contain gases or air such as the lungs.
- The quality of an ultrasound diagnosis depends on where the scan cut is set.
 - Before starting an exam, carefully consider where to set the plane for scanning with the transducer so that the area of interest can be accurately located using ultrasound.

• If you have any questions or suggestions about this diagnostic system please contact TELEMED Company.

NOTES:



The term "Acquisition" used here refers to the image forming process whereby a picture is displayed on the monitor screen as a result of emitting ultrasound waves and receiving echoes by the ultrasound transducer. Both the transmitter and the receiver are activated during this acquisition process.

The term FREEZE refers to the stoppage of the acquisition. FREEZE button turns off the ultrasound transducer circuit.

5.2. Getting Started

Recommended Windows PC configuration:

- Microsoft Windows compatible Desktop/Notebook/Tablet PC
- Intel chipset-based motherboard with at least one integrated USB 3.0 port available
- CPU Intel Core i5/i7 1.8 GHz or faster
- 2 GB of RAM or more
- NVIDIA graphic card, 256 Mb, CUDA 2.3 support
- TCO certified monitor with screen resolution 1024x768 or more, IPS or PLS technology
- Certified for medical use computer power supply
- Microsoft Windows® 7, Windows® 8, Windows® 10 (all versions 32/64-bit) operating system

Before installation please read information from web:

ftp://pcultrasound.com/Public/Software/TELEMED%20Drivers%20Pac kage/readme.txt

ftp://pcultrasound.com/Public/Software/Echo%20Wave%20II%20LB2/
readme.txt

Refer to:

- ECHO WAVE II Operation Manual
- ArtUs User Guide
 - Chapter 2.5 Cybersecurity
 - Chapter 5.3 Windows configuring
- 1. Connect the power supply and USB cable. Insert the transducer connector into the socket firmly until it locks with spring latches please refer to the picture below (according to configuration of **ArtUs EXT-1H**).



- 2. Switch on the computer power and wait until Windows is ready.
- 3. Start Echo Wave II application.

Note: For USA market by FDA recommendation the system performs transducer elements check each time when transducer is connected to the system or activated. If a critical amount of unresponsive elements is found during the element check procedure the system will pop up the warning message describing the problem. In this case the user can try to re-connect the transducer. If the problem persists the user should contact technical support.

Note: Please observe the battery status (charging, battery volume etc.) in the Windows system tray. If the system is battery powered, a warning will be displayed on the screen when only 15% is remaining. In such case you should charge the system before continuing to use.

5.3. Ultrasound Scanner Monitor utility

Ultrasound Scanner Monitor utility is used for system status monitoring. In addition, this utility helps to see when and how the **ArtUs** is connected to the computer and to view the generated Log file.

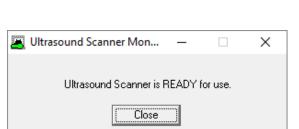
- Utility icon is located in the Windows system tray bar; here shown system tray image corresponds to Windows 10, in other Windows versions it may slightly differ;
- When the icon is highlighted in RED — the drivers for the **ArtUs** beamformer have not been installed properly or the beamformer is not connected to the USB port;

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14:27

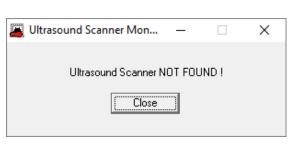
2018-10-18

- When the icon is highlighted in GREEN the drivers for the **ArtUs** beamformer are properly installed and the beamformer is connected to the USB port and the system is ready to start;
- Using the left mouse button double click on the GREEN highlighted Ultrasound Scanner Monitor icon and this message will appear;



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- Using the left mouse button double click on the RED highlighted Ultrasound Scanner Monitor icon and this message will appear;
- By clicking with the right mouse button on the Ultrasound Scanner Monitor icon an additional menu will appear;



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About		
Show Log		
Exit	14:37	
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About		
Show Log		
Exit	14:38	
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About		
About Show Log		
	14:38	
Show Log	14:38 2018-10-18	
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• By clicking on the left mouse button, you can select About, Show Log and Exit menu items;



NOTE:

Do not unplug the power cable during the scan mode. Doing this may cause damage to the scanner. Exit the software and only

unplug the power cable once this has been done.

5.4. Windows Configuring

5.4.1. E-mail

Configure the E-mail program (for example, Microsoft Outlook Express, Mozilla Thunderbird). It is necessary for normal operation of the direct E-mail sending feature of the ultrasound software.

Note: There is no need to configure the E-mail software if you are not planning to use it or if your computer is not currently connected to the Internet.

5.4.2. Windows account

For each system user Windows account with separate login and password must be created.

- Create a local user account https://technet.microsoft.com/enus/library/cc770642(v=ws.11).aspx
- Create a user account in Windows https://support.microsoft.com/en-us/help/13951/windowscreate-user-account
- User Accounts https://technet.microsoft.com/en-us/library/dd277409.aspx

5.4.3. Windows security

It is strongly recommended that in Windows security will be strengthened using Security Policy Settings and monitored using Windows Security Audit.

- How to Configure Security Policy Settings https://technet.microsoft.com/enus/library/dn135243(v=ws.10).aspx
- Security Auditing Overview https://technet.microsoft.com/enus/library/dn319078(v=ws.11).aspx

5.4.4. Antivirus

It is strongly recommended that on computers will be installed antivirus software, for example, Microsoft Security Essentials, Windows Defender, and will be turned on its updates.

Microsoft Security Essentials Download

https://support.microsoft.com/en-us/help/14210/securityessentials-download

• Windows Defender

https://support.microsoft.com/en-us/help/17464/windowsdefender-help-protect-computer

• Updating your Microsoft antimalware and antispyware software https://www.microsoft.com/security/portal/definitions/adl.a spx

5.4.5. Firewall

It is strongly recommended that on computer will be turned on Windows Firewall.

• How to Configure Windows Firewall on a Single Computer https://msdn.microsoft.com/en-us/library/cc875811.aspx

5.4.6. Windows updates

It is strongly recommended that computers will have turned on Windows Updates.

• Windows Update: FAQ https://support.microsoft.com/en-us/help/12373/windowsupdate-faq

5.4.7. Network communication

It is strongly recommended that for network communication will be used secure Virtual Private Networks (VPN).

• Virtual Private Networks https://technet.microsoft.com/en-us/library/cc977889.aspx

5.4.8. Digital Signature

Ultrasound software distribution packages (setup(s)) and essential ultrasound software parts (drivers) are digitally signed.

This means that the user can check file properties and see if file signature (digital certificate) is valid and what company signed that file. 64-bit Windows operating systems does not load drivers that do not have signature or signature is invalid. This means that ultrasound scanning will not be started (driver will not be loaded) if it is modified by any malware.

• Digital Signatures for Kernel Modules on Systems Running Windows Vista https://msdn.microsoft.com/en-us/library/bb530195.aspx

```
• Digital signatures and certificates
https://support.office.com/en-us/article/Digital-
signatures-and-certificates-8186cd15-e7ac-4a16-8597-
22bd163e8e96
```

5.4.9. Windows AppLocker

It is strongly recommended that in Windows will be configured what applications can be run by what user(s) by using Windows AppLocker.

```
• Windows AppLocker
https://technet.microsoft.com/en-
us/library/dd759117(v=ws.11).aspx
```

5.4.10. Encrypted file system

It is strongly recommended that computer data will be protected by using encrypted file system.

- The Encrypting File System https://technet.microsoft.com/en-us/library/cc700811.aspx
- BitLocker https://technet.microsoft.com/library/cc732774.aspx

5.5. Finishing Work

To finish work please follow the instructions below:

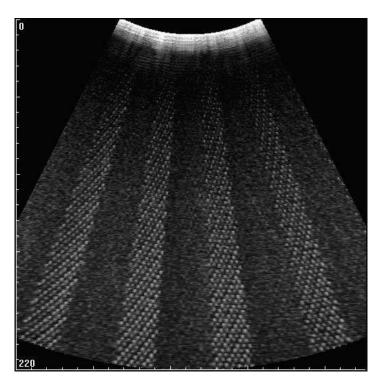
- 1. Exit EchoWave II application.
- 2. Disconnect power plug from the device.
- 3. Disconnect the transducer(s) from the device and follow the cleaning and disinfection procedures.
- 4. Disconnect USB cable (if needed).
- 5. Power off the computer (if needed).

6. TROUBLESHOOTING

Read this chapter carefully before calling the Technical Support service.

6.1. FAQ

Question: An increased level of noise and interference is observed on ultrasound images as shown at image below. What do I need to do in order to reduce the noise levels?



Answer: The reason for this appearance may be electronic equipment and devices which emit this type of electromagnetic noises. Please position ultrasound scanner, ultrasound transducer and its cable at some distance from such equipment.

Question: Connected and powered device does not enter scanning mode (no ultrasound image in EchoWave II application). What can be a reason?

Answer: Possible cause can be that device is waiting for external synchronization signal. This mode of operation can be switched off using **ArtUs Sync Options.exe** utility. The utility package can be found here:

ftp://pcultrasound.com/Public/Software/Synch package/

Please run the utility and switch off external synchronization options.

6.2. Contact with technical support service

If you encounter problems during the installation or during operation and you are still unable to solve them contact us via the support@pcultrasound.com e-mail address. First please send to technical support service the following information:

- Scanner type (for example: ArtUs EXT-1H);
- Serial number of the scanner (for example: 2351-120428-9686);
- Transducer type (for example: C5-2H60-A5);
- Serial number of the *transducer* (for example: 3241-120504-9701);
- TELEMED Drivers Package version (for example: TELEMED Drivers Package 1.17.3);
- Echo Wave II software version (for example: Echo Wave II 3.7.1);
- Attached Log file generated by scanner (see section "Ultrasound Scanner Monitor Utility")
- Also please start sysinfo.exe utility from Echo Wave II installation folder, wait while it generates a log file and send this log file to us. Usually the path to sysinfo.exe utility is as follows:

"C:\Program Files (x86)\TELEMED\Echo Wave II\sysinfo.exe" (on 64-bit Windows)

"C:\Program Files\TELEMED\Echo Wave II\sysinfo.exe" (on 32-bit Windows)

7. WARRANTY AND SERVICE INFORMATION

7.1. Warranty

TELEMED guarantees that the diagnostic system is free from defects regarding materials and workmanship at the original purchaser's location for a period of 24 months (the one exception being the transducer which is guaranteed for 18 months). This guarantee or warranty covers parts for the full 24 months (or 18 months for transducers) and labor for 90 days. In order to comply with this warranty, all service must be performed by a TELEMED qualified field engineer or only with the express permission of TELEMED. Items not included in this warranty are misuse, negligence or accidental damage. TELEMED wishes to point out that the loss of data loss is not included in this guarantee.

The foregoing warranty is exclusive of and in lieu of all other warranties and representations, expressed or implied, including but not limited to any warranty of merchantability or fitness for any particular trade usage. This warranty is also in lieu of any other obligations, liabilities, rights or claims, whether included in the contract or not, including any rights arising from negligence on the part of TELEMED for any direct, incidental, consequential or any other damages.

7.2. Warranty Shipments and Returns

- A warranty claim must be made without delay and must be received during the applicable warranty (guarantee) period by TELEMED.
- If it is necessary to return a product for repair and/or adjustment, prior authorization from TELEMED must be obtained first. Instructions as to how and where these products should be shipped will be provided by TELEMED.
- Any product or component returned for examination and/or warranty repair shall be sent insured and prepaid via the means of transportation specified by TELEMED. Shipping charges for all products or components replaced or repaired under warranty should be defined separately.
- In all cases, TELEMED has sole responsibility for determining the cause and nature of failure, and TELEMED decisions with regard to this shall be final.

7.3. Service Contract

A service contract may be obtained for the TELEMED after the original warranty or guarantee period has expired. The contract provides for any service calls that may be necessary to keep the system operational and will include at least one regularly scheduled service visit per year. As part of the scheduled maintenance, the service representative will do a complete inspection and test / calibration of the system.

To help us provide our customers with the best possible support please send your comments and suggestions to support@pcultrasound.com

8. MAINTENANCE

Performance and Safety Checks see in the table below:

Recommended Maintenance	Frequency
General cleaning	As Need
Inspect the system, cables and transducers	Before Use/Daily
System accuracy and performance verification	Annually

8.1. General cleaning

The LCD/CRT screen and all external surfaces can be cleaned with a soft cloth dampened with a neutral detergent. Do not use solutions containing chlorine, ammonia, fluoro-carbons or hydro-carbons. Do not use abrasive cleaners or fibrous wipes that may scratch the surface.



<u>NOTE:</u> Before cleaning the unit, ensure that the unit is turned off and the mains power cable is disconnected.

8.2. Inspecting the System

Examine the exterior for cleanliness and general physical condition. Ensure that the housing is intact, all hardware is present and secure and that the labeling is legible.

Check the cables (especially power cable). If there is any peeling or cracking of the outside insulation carefully disconnect the cable and replace it with a new one.

8.3. Transducers maintenance and disinfection

All transducers are supplied as non-sterile.

Transducers in Endocavity Procedures should normally be used with a sterile sheath.

Transvaginal transducers may be used with a surgically clean sheath.

The following disinfectants have been tested with your transducers.

Use of any other disinfectants may void the system warranty (guarantee) and service contract.

The following disinfectants are recommended for soaking or wiping:

Transducer model	Compatible disinfectant
BIPC6.5/10/128Z-4 + BIPL7.0/60/128Z-4 BIPC8-4R10N-4 + BIPL10-4L60N-4 BIPC9-4R10H-4 + BIPL12-5L70H-4 HL9.0/40/128Z-4 L12-5L40N-4 L15-6L25N-4 L18-10L30H-4 MC10-4R12N-4	Cidex Plus, Cidex OPA, Anioxyde 1000, 75% IPA, Sani-cloth bleach, Metricide OPA plus, Rely+On PeraSafe, Cydezyme XTRA, Cleansept Wipes, Nu-Cidex, Alkazyme, Steranios 2%, Salvanios PH10, Cidex 2%, Klenzyme, Revital-Ox Resert
C3.5/20/64D-3, C3.5/20/128Z-3 C3.5/60/64D-3, C3.5/60/128Z-3 C5-2R60S-3, EC6.5/10/64D-3 EC6.5/10/128Z-3, HL9.0/40/64D-3 L12-5L40S-3, L12-5N40-M3 L15-6L25S-3, LF9-5N60-A3 LF11-5H60-A3, LV7.5/65/64D-3 LV8-4L65S-3, MC4-2R20S-3 MC8-4R20S-3, MC10-5R10S-3 MCV9-5R10N-3, MCV9-5N10-A3 MCV9-5R10S-3, PV6.5/10/64D-3 PV6.5/10/128Z-3	Cidex OPA, Cidex Plus, INCIDIN OXYFOAM
C4.5/50/128Z-2, HL9.0/60/128Z-2 LV7.5/60/128Z-2, LV8-5L60N-2 LV8-5N60-A2	ENZOL, Cidex OPA
C5-2H60-A5, C5-2R60HI-5 C5-2R60NI-5, C6-1H50-A5 C7-3R50NI-5, L15-7H40-A5 L15-7L40H-5, L18-7H30-A5	Cidezyme / Enzol, MetriZyme, Cidex OPA, Cidex Plus, Sterihyde, Osvan (10%/V%), Neojodin Solution, Milton, Hibitane (5% Chlorhexidine gluconate)
P5-1L15SI-6 P5-1S15-A6 P8-3L10SI-6	ANIOS, Aquasonic 100 Gel, Cidex OPA, ENZOL, Gigasept FF, Klenzyme, MetriZyme, Milton, SANI-CLOTH HB, SPOROX 2, Super SANI-CLOTH, T-Spray, Transeptic Spray, Virkon S, Wavicide-01, Cidex Plus

NOTE:



Among the above-listed disinfectants, High level disinfectants can be applied to Endocavity transducer, however Low-level disinfectants are not appropriate for disinfection of Endocavity transducer.

CAUTION: Customers must follow the disinfectant manufacturer instructions carefully.

Do not submerge transducers above strain relief.

8.3.1. Chemicals that Damage Transducers:

WARNING:



Some of chemicals, such as phenol, benzethonium chloride, hexachlorophene (Phisohex), benzoyl peroxide, hydrogen peroxide, are commonly found in clinics or hospital settings while others are often found in antibacterial skin cleaners or lotions. Use of these chemicals will cause damage to a transducer. This damage is not covered by the warranty or service contract.

8.3.2. Recommended Procedures for Transducer Processing

Inspect the transducer cable, connector and the lens surface. Contacts on the transducer connector must not be bent. The surface of transducer lens must be clean without any remnants left. Check for any cracks which might allow liquids to enter the transducer (especially joints such as cable/connector and cable/transducer). If any such damage is found, do not use the transducer until it is replaced.

Use care to avoid getting solution in the transducer connector. Wrap the connector in the plastic bag to avoid contact between liquids and the connector.

Use an EPA registered germ killer intended for use on plastic medical instruments (2% Glutaraldehyde type solutions without surfactants are recommended). Follow the germ killer manufacturer's instructions regarding concentration, contact duration and storage and disposal.

Do not use alcohol or alcohol-based solutions. Thoroughly rinse all residues from the transducer using sterile distilled water after removal from the germ killer. Do not wipe the strain relief/housing joint, the strain relief, or the cable with isopropyl alcohol. Isopropyl alcohol can cause damage to these parts of the transducer. This and any mechanical damage are not covered by the warranty or your service contract.

8.3.3. General Cleansing for Transducers Used in Non-Invasive Procedures

These general cleaning instructions are recommended for non-critical category transducers.

All transducers which do not come into contact with mucus membranes, blood, compromised tissue and which are not used in sterile fields can be cleaned by following these instructions. It is important that customer cleans the transducer and cable according to the following procedures:

1. Wipe the ultrasound transmission gel off the transducer after every patient exam.

2. Wipe the transducer and cable with a dry or water-moistened soft cloth.

3. Wipe the transducer with any recommended disinfectant.

4. It is also possible to wipe the cable with T-spray, a low-level disinfectant for the cleaning of external transducers only. You are not allowed to use isopropyl alcohol on the cable and strain relief/housing joint.

8.3.4. Cleansing and Disinfection of Transducers Used in Endocavity Procedures

It is highly recommended to use Transducer's Sheaths for Endocavity and Invasive uses.

The transducer disinfection should be done prior to the first exam, and following every exam thereafter.

The disinfectant procedure includes the following steps:

1. Unplugging the transducer from the system.

2. Washing the transducer head and cable with soap and water to remove any protein buildups but the transducer however must not be rinsed or immersed near the strain relief.

3. Disinfection of the transducer and the cable with one of the disinfectants listed as Legally Marketed. During the disinfection it is necessary:

- avoid transducer contact with strong solvents such as acetone, freon, and other industrial cleansers
- avoid soaking the transducer for extended periods of time, such as overnight
- avoid rinsing or immersing near the strain relief.

4. Removing the transducer from the disinfectant and thoroughly rinsing with sterile water.

5. Checking the transducer for any residual organic material. If any materials are present the disinfection of the transducer should be done again.

8.4. System Accuracy / Performance Verification

System accuracy and performance verification should be conducted annually or if any doubts exist about image quality or distance estimation.

Use tissue mimicking phantoms for evaluation of accuracy and performance of the system. Refer to the Manual supplied with the phantom for detailed description of accuracy and performance verification.

During the performance assessment or tests (using phantoms etc.) the transducer lens may be immersed in water or other special liquid for a short period of time (but not above strain relief).



<u>NOTE:</u>

The System was designed for sound velocity in tissues at 1540 m/sec. For accuracy verification phantoms which have been calibrated for this sound velocity should be used.

9. TRANSPORTATION, STORAGE AND UTILIZATION

9.1. Transportation and storage

The ultrasound scanner should be stored and moved according to the package technical documentation and the standard procedures.

9.2. Disposal

Disposal/recycling of this equipment should be carried out by a specialized company and be performed in accordance with local laws and legislation.

10. DECLARATION OF CONFORMITY

DECLARATION OF CONFORMITY

We,

TELEMED UAB

Highway Business Centre Savanoriu pr. 178A Vilnius LT-03154 Lithuania

Declare under our sole responsibility that:

Equipment	Ultrasound scanners	Probes	
	ArtUs EXT-1H	C5-2H60-A5	P5-1S15-A6
	ArtUs EXT-2H	L12-5N40-A4	LF9-5N60-A3
		L15-7H40-A5	LF11-5H60-A3
		L18-7H30-A5	MCV9-5N10-A3

Software Echo Wave II

Classification: Class IIa (in compliance with Annex II, Art 11 Medical Device Directive) are in conformity with:

Essential Requirements of Council Directive 93/42/EEC (Medical Device Directive)

IEC 60601-1: 2006/A1:2012, Part 1: General requirements for basic safety and essential performance.

IEC 60601-1-2: 2014, Part 1: General requirements for basic safety and essential performance, 2. Collateral standard: Electromagnetic compatibility - Requirements and tests

IEC 60601-2-37:2015 Particular requirements for the basic safety and essential performance of ultrasonic medical diagnostic and monitoring equipment

ISO-10993-1:2009, Biological Evaluation of Medical Devices, Part 1: Evaluation and Testing within a risk management process.

ISO 10993-5:2009 Biological evaluation of medical devices -- Part 5: Tests for in vitro cytotoxicity

ISO-10993-10:2010, Biological Evaluation of Medical Devices, Part 10: Tests for irritation and skin sonsitization

IEC 62304: 2006/A1:2015 Medical device software -- Software life cycle processes

ISO 14971:2012 Medical devices -- Application of risk management to medical devices

IEC 62366-1:2015 Medical devices -- Part 1: Application of usability engineering to medical devices

ISO 15223-1:2016 Medical devices -- Symbols to be used with medical device labels, labelling and information to be supplied -- Part 1: General requirements

The compliance with the Council Directive 93/42/EEC is under the monitoring of the Notified Body: MEDCERT GmbH Pilatuspool 2 20355 Hamburg, code: 0482

Date of issua. C8 July 2021

Dmitry Novikov, President

11. <u>APPENDICES</u>

11.1. Guidelines for the safe use of diagnostic ultrasound

• Recommendations

General

- The use of diagnostic ultrasound to obtain information about functions or structures in human beings should be restricted to situations in which the medical benefit that may accrue from the diagnostic data outweighs any foreseeable risk. Most such situations are limited to clinical examinations of the ill or potentially ill patient or pregnant women.
- Situations such as training, demonstrations or research may also provide a medical benefit from diagnostic data and one that outweighs any foreseeable risk. Here, information is obtained for people who are not necessarily in the categories of Recommendation (1), above. During all training, demonstration or research situations, if either the Thermal Index or the Mechanical Index exceeds 1, then a subject should be informed of the anticipated exposure condition and how it compares regarding safety with conditions for normal diagnostic practice.
- Ultrasound should not be used for any of the following:
- obtaining pictures of the fetus solely for non-medical reasons;
- learning the sex of the fetus solely for *non-medical* reasons;
- for commercial purposes, such as trade shows, or producing pictures or videos of the fetus.

Thermal Effects

- The M-mode is a valuable clinical tool and, despite any potential risks, is not contraindicated. Operators however should be careful to limit exposure to only vital structures and utilize the exposure information provided by the manufacturer.
- In particular, users should employ exposures which are As Low As Reasonably Achievable (ALARA)¹ because of the potential for ultrasonic heating of tissues during M-mode imaging and, normally to a significantly greater extent, Doppler ultrasound blood flow examinations. Exposure can be reduced by either reducing the Thermal Index using the output controls or by reducing the dwell time which is the amount of time that the transducer remains in any one place.

Mechanical Effects

- Users should employ exposures, regardless of the mode used, which are **As Low As Reasonably Achievable (ALARA)** because of the potential for:
- ultrasonically induced capillary hemorrhaging in lung tissues if it is exposed during pediatric diagnostic ultrasound examinations, particularly in the case of infants and neonates and especially if they are pre-term;

- ultrasonically induced capillary hemorrhaging of the intestine where intestinal peristalsis is inhibited or conditions promote intraluminal or sub-mucosal gas collections;
- ultrasonically induced capillary hemorrhaging in other soft tissues when Gas Contrast Agents are used.
- Use of Gas Contrast Agents during a diagnostic ultrasound examination is not recommended within 24 hours before extracorporeal shock wave lithotripsy.
- Exposure can be reduced by lowering the **Mechanical Index** using the output controls. Reducing the **dwell time** is of use if threshold pressures are exceeded.

Quality Assurance

It is recommended that equipment operators implement quality assurance measures to maintain the capability of obtaining reliable diagnostic information at acoustic exposures which are **As Low As Reasonably Achievable**.

Since the quality of diagnostic information depends, in part, on operator training, it is also recommended that sonographers (ultrasound technologists) are appropriately qualified and registered in regional organizations of ultrasound professionals.

Conclusions

General

- Although there are many exposure conditions for which the risk of injury during a diagnostic ultrasound examination is negligible, this is not the case for every possible exposure condition using currently available equipment. Therefore, the persons responsible for the ultrasonic exposure must ensure that the exposure is justified, i.e. that reliable diagnostic information can be achieved and that the benefits significantly outweigh the risk involved
- The conclusions listed below provide guidance as to the risks due to thermal and mechanical effects resulting from ultrasound exposure. To be useful, all the conclusions need to be taken into consideration.

Thermal Effects

- At the time of writing, the information published on output levels during B-mode imaging indicates that the risk of injury from **ultrasonic heating** is negligible during this type of examination. At this time, there appears to be no reason based on thermal grounds to limit such scanning for any clinical indication, including ultrasound examination of normally pregnant women.
- In all other operating modes, especially those used for Doppler blood flow examinations, the risk of injury from **ultrasonic heating** depends on the temperature elevation and the **dwell time** as indicated by the conclusions given below.
- If the **Thermal Index (TI)** does not exceed 1, currently available evidence indicates that the risk of an injury due to **ultrasonic heating** is negligible for the vast majority of conditions of the diagnostic ultrasound examination.
- During the first trimester, and in the case of trans-abdominal fetal examinations through a bladder path greater than 5 cm in length, current evidence indicates that it is possible that the maximum temperature elevation which could be

obtained is as much as 2-3 times that of the displayed **Soft Tissue Thermal Index (TIS)**. More caution may be warranted in these situations, particularly if the **TIS** exceeds 1.

- The **Soft Tissue Thermal Index (TIS)** is the appropriate indicator of the potential for **ultrasonic heating** for examinations in which the ultrasound beam travels a path which is principally made up of homogeneous soft tissue or a soft tissue/fluid path, as during a first trimester fetal examination or an abdominal examination.
- If bone, including 2nd or 3rd trimester fetal bone, is within the ultrasound beam the **Bone Thermal Index (TIB)** is often the appropriate indicator, except as noted in the next conclusion.
- If bone is in contact with the transducer the **Cranial Thermal Index (TIC)** is the appropriate indicator. If bone is within approximately 1 cm of the transducer and this is closer than the nearest focal zone, the **Cranial Thermal Index (TIC)** is the appropriate indicator. More caution may be warranted in these cases because of the potential for transducer self-heating and heating of the transducer may add significantly to any **ultrasonic heating** which may occur.
- Generally, more caution may be warranted for transvaginal, transesophageal and transrectal examinations because heating of the transducer may potentially produce additional heat to adjacent tissue.
- This conclusion and the following one provide guidance to the user if the temperature elevation in the fetus can possibly exceed 1 °C as a result of a diagnostic ultrasound exposure. If the exposure produces a maximum *in situ* temperature of no more than 38.5 °C (1.5 °C above normal physiological levels) then it may be used clinically without reservation on thermal grounds.
- To be considered potentially hazardous on thermal grounds, it appears that a diagnostic ultrasound exposure must elevate embryonic and fetal *in situ* temperatures to the following temperatures for approximately the corresponding durations:
 - 39 °C, (2 degrees above normal), 60 minutes;
 - 40 °C, (3 degrees above normal), 15 minutes;
 - 41 °C, (4 degrees above normal), 4 minutes;
 - 42 °C, (5 degrees above normal), 1 minute;
 - 43 °C, (6 degrees above normal), 0.25 minutes.

Mechanical Effects

- At exposures that do not exceed the output limits recommended in the section entitled **Thermal effects**, there is no demonstrated risk of clinically significant damage in humans from the mechanical effects of ultrasound exposure during a diagnostic examination. However, capillary hemorrhaging has been observed in lungs and in the intestine of mammals at diagnostically relevant exposures. This effect has also been observed in other soft tissues if gas contrast agents are used. For the most part, thresholds are just as likely to be exceeded for B-mode as for pulsed Doppler or color flow Doppler modes. However, thresholds are lower for pulsed Doppler modes with relatively long pulses.
- If the **Mechanical Index (MI)** exceeds 1, there is a small risk of capillary hemorrhaging in the lung during ultrasound examinations involving exposure of the neonatal and infant chest. The risk may increase in more unusual exposures where the surface of the lung is near the focus. Although clinically significant hemorrhaging is unlikely, in part because of the small volume of tissue affected,

the potential for achieving clinical significance may increase in premature infants.

- At the current maximum values for the **MI** of 1.9, it is unlikely that diagnostic ultrasound exposure could lead to clinically significant intestinal hemorrhaging in human beings. However, this likelihood may increase for pathologic conditions inhibiting intestinal peristalsis and promoting intraluminal and sub-mucosal gas collections.
- A limited number of experimental studies suggest that the use of ultrasound gas contrast agents (GCAs or micro bubbles) during a diagnostic examination may potentially increase the likelihood of capillary hemorrhaging in tissues other than lung tissue. In animal experiments, the risk of significant hemorrhaging from lithotripter fields is increased for several hours after injection.
- As long as the recommended output limits are not exceeded, mechanical effects are far less likely to be important in obstetrical ultrasound because of the absence of gas bodies.

Biological Effects

The clinical effect of exposure depends on the nature and degree of tissue injury. This can be assessed from biological effects studies. Several extensive reviews have been published regarding the adverse biological effects of **ultrasonic heating** based on animal studies, particularly in mammalian species (Lele 1985, NCRP 1992, WFUMB 1992, AIUM 1993, WFUMB 1998). With regards to adult tissues, the available literature suggests that tissue temperature elevations in the range of 8-10 °C, sustained for 1 to 2 minutes will cause tissue injury (Bly, *et al.*, 1992, Lele 1985).

The reviews have also considered studies of teratogenic effects, usually on the developing brain, due to whole body heating of the embryo or fetus. The recommendations resulting from these reviews can be succinctly expressed as follows (WFUMB 1998):

- a diagnostic ultrasound exposure that produces a maximum *in situ* temperature rise of no more than 1.5 °C above normal physiological levels (37 °C) may be used clinically without reservation on thermal grounds,
- a diagnostic ultrasound exposure that elevates embryonic and fetal *in situ* temperature above 41 °C (4 °C above normal temperature) for 5 minutes or more should be considered potentially hazardous,
- the risk of adverse effects is increased with the duration of exposure.

In addition, it has been reported that water immersion body heating of rats resulted in the development of encephaloceles in the rat fetuses following as little as 1 minute at a temperature elevation of 5 °C above normal physiological temperature. (WFUMB 1998).

For temperature elevations greater than 1.5 °C above normal physiological levels (37 °C), this information can be approximately matched to a functional form recommended by the NCRP (NCRP 1992). This yields an equation for combinations of temperature elevation and time which should be considered potentially hazardous:

 $t = 4^{5-\Delta T}$

where it is the time in minutes at the specified temperature and ${}^{\Delta T}$ is the temperature elevation above normal (37 °C).

Barnett, et al., (1997) have recently published an updated review of thermal effects, focusing on the potential for effects on the fetus. They note that there is little information on the teratogenic effects from localized heat damage caused by ultrasound.

References

Abbott, JG. Rationale and derivation of MI and TI - a review. Ultrasound in Med. and Biol. 25:431-441; 1999.

American Institute of Ultrasound in Medicine (AIUM). Bioeffects and safety of diagnostic ultrasound. Laurel, MD: AIUM Publications; 1993.

American Institute of Ultrasound in Medicine/National Electrical Manufacturers Association (AIUM/NEMA). Standard for real-time display of thermal and mechanical acoustic output indices on diagnostic ultrasound equipment, Revision 1. Laurel, MD: AIUM Publications; 1998a.

American Institute of Ultrasound in Medicine/National Electrical Manufacturers Association (AIUM/NEMA). Acoustic output measurement standard for diagnostic ultrasound equipment. Laurel, MD: AIUM Publications; 1998.

American Institute of Ultrasound in Medicine (AIUM). Medical ultrasound safety. Rockville, MD: AIUM Publications; 1994.

American Institute of Ultrasound in Medicine (AIUM). Standard Methods for Measuring Performance of Pulse Echo Ultrasound Imaging Equipment. Rockville, MD: AIUM Publications; 1991.

American Institute of Ultrasound in Medicine (AIUM). Methods for Measuring Performance of Pulse-Echo Ultrasound Equipment, Part II: Digital Methods. Rockville, MD: AIUM Publications; 1995a.

American Institute of Ultrasound in Medicine (AIUM). AIUM Quality Assurance Manual for Gray-Scale Ultrasound Scanners. Rockville, MD: AIUM Publications; 1995b.

American Institute of Ultrasound in Medicine (AIUM). Mechanical Bioeffects from Diagnostic Ultrasound: AIUM Consensus Statements. J. Ultrasound in Medicine 19: number 2; (February 2000). (Also available from AIUM Publications.)

Apfel, R.E. and Holland, C.K. Gauging the likelihood of cavitations from short-pulse, low duty cycle diagnostic ultrasound. Ultrasound in Med. and Biol. 17:179-185; 1991.

Barnett, S.B., ter Haar, G.R., Ziskin, M.C., Rott, H.D., Duck, F.A. and Maeda, K. International recommendations and guidelines for the safe use of diagnostic ultrasound in medicine. Ultrasound in Med. and Biol. 26:355-366; 2000.

Bly, S.H.P., Vlahovich, S., Mabee, P.R. and Hussey, R.G. Computed estimates of maximum temperature elevations in fetal tissues during transabdominal pulsed Doppler examinations. Ultrasound in Med. and Biol. 18:389-397; 1992.

Carstensen, E.L., Duck, F.A., Meltzer, R.S., Schwarz, K.Q., Keller, B. Bioeffects in echocardiography. Echocardiography 6:605-623; 1992.

Child, S.Z., Hartman, C.L., McHale, L.A and E.L. Carstensen. Lung damage from exposure to pulsed ultrasound. Ultrasound in Med. and Biol. 16:817-825; 1990.

Dalecki, D., Raeman CH, Child SZ, *et al*, . The influence of contrast agents on hemorrhage produced by lithotripter fields. Ultrasound in Med. and Biol. 23:1435-1439; 1997.

Doody, C. Porter, H., Duck, F.A. and Humphrey, V.F. *In vitro* heating of human fetal vertebra by pulsed diagnostic ultrasound. Ultrasound in Med. and Biol. 25:1289-1294; 1999.

Duck, F.A., Starritt, H.C., ter Haar, G.R. and Lunt, M.J. Surface heating of diagnostic ultrasound transducers. Br. J. Radiology 67:1005-1013; 1989.

Duggan, P.M. and McCowan, L.M.E. Reference Ranges and Ultrasonographic Exposure Conditions for Pulsed Doppler Sonographic Studies of the Fetal Internal Carotid Artery. J Ultrasound in Medicine 12:719 - 722; 1993.

Henderson, J., Willson, K., Jago, J.R. and Whittingham, T. A survey of the acoustic outputs of diagnostic ultrasound equipment in current clinical use. Ultrasound in Med. and Biol. 21:699-705; 1995.

Holland, C.K., Deng, C.X., Apfel, R.E., Alderman, J.L., Fernandez, L.A., and Taylor, K.J.W. Direct evidence of cavitation *in vivo* from diagnostic ultrasound. Ultrasound in Med. and Biol. 22:917-925; 1996.

Lele, P.P. Local hyperthermia by ultrasound for cancer therapy. In: Nyborg, W.L.; Ziskin, M.C., eds. Biological effects of ultrasound. Clinics in diagnostic ultrasound, Vol.16. New York: Churchill Livingstone: 135-155; 1985.

Lopez, H. How to Interpret the Ultrasound Output Display Standard for Higher Acoustic Output Diagnostic Ultrasound Devices. J. Ultrasound in Medicine, Vol 17, pg 535 (1998).

Miller, D.L. and Gies, R.A. Gas-body-based contrast agent enhances vascular bioeffects of 1.09 MHz ultrasound on mouse intestine. Ultrasound in Med. and Biol. 24:1201-1208; 1998.

National Council on Radiation Protection and Measurements (NCRP). Exposure criteria for medical diagnostic ultrasound: I. Criteria based on thermal mechanisms. Bethesda, MD: NCRP; June 1, 1992.

National Council on Radiation Protection and Measurements (NCRP). Exposure criteria for medical diagnostic ultrasound: II. Criteria based on mechanical mechanisms. Bethesda, MD: NCRP; in preparation

O'Neill, T.P., Winkler, A.J. and Wu, J. Ultrasound heating in a tissue-bone phantom. Ultrasound in Med. and Biol. 20:579-588; 1994.

Patton, C.A., Harris, G.R. and Phillips, R.A. Output Levels and Bioeffects Indices from Diagnostic Ultrasound Exposure Data Reported to the FDA. IEEE Trans Ultras Ferro, Freq Cont 41:353-359; 1994.

Ramnarine, K.V., Nassiri, D.K., Pearce, J.M., Joseph, A.E.A., Patel, R.H. and Varma, T.R. Estimation of *in situ* ultrasound exposure during obstetric examinations. Ultrasound in Med. and Biol. 19:319-329; 1993.

Shaw, A., Preston, R.C. and Bond, A.D. Assessment of the likely thermal index values for pulsed Doppler ultrasonic equipment - Stage I: calculation based on manufacturers' data. NPL Report CIRA (EXT) 018; 1997.

Shaw, A., Pay, N.M. and Preston, R.C. Assessment of the likely thermal index values for pulsed Doppler ultrasonic equipment - Stages II and III: experimental assessment of scanner/transducer combinations. NPL Report CMAM 12; 1998.

Siddiqi, T.A., O'Brien, W.D., Meyer, R.A., Sullivan, J.M. and Miodovnik, M. *In situ* human obstetrical ultrasound exposimetry: estimates of derating factors for each of three different tissue models. Ultrasound in Med. and Biol. 21:379-391; 1995.

U.S. Food and Drug Administration (FDA). Information for manufacturers seeking marketing clearance of diagnostic ultrasound systems and transducers. Rockville, MD: FDA; Sept 30, 1997.

World Federation for Ultrasound in Medicine and Biology (WFUMB) WFUMB Symposium on Safety and Standardization in Medical Ultrasound, Chapter 1, ed., Barnett, S.B. and Kossoff, G. Ultrasound in Med. and Biol. 18:739-750; 1992.

World Federation for Ultrasound in Medicine and Biology (WFUMB) WFUMB Symposium on Safety of Ultrasound in Medicine. Conclusions and recommendations on thermal and non-thermal mechanisms for biological effects of ultrasound. ed., Barnett, S.B. Ultrasound in Med. and Biol. 24: Supplement 1, 1998.

Glossary of Terms

ALARA (As Low As Reasonably Achievable): a principle which is used to reduce any unnecessary and potentially hazardous exposure to individuals by keeping doses As Low As Reasonably Achievable.

As shown throughout this guideline, application of the ALARA principle to diagnostic ultrasound differs from its common usage in diagnostic X-ray imaging where it is assumed that there is no threshold exposure.

In the use of diagnostic ultrasound, there are three ranges of exposure, i.e. combinations of Thermal or Mechanical Indices and dwell time that need to be considered. At exposures that are clearly below the thresholds for health effects, further reduction of exposure is not justified, whether it is via reductions in dwell time or acoustic output. There can also be exposure that is or may be above thresholds for health effects. In these cases, ALARA refers to using the lowest value of potentially hazardous exposure, i.e. a combination of acoustic output and dwell time needed to achieve the required diagnostic information.

Bone Thermal Index (TIB): The Thermal Index for an exposure model in which the ultrasound beam passes through soft tissue and a focal region is in the immediate vicinity of bone.

Cranial Bone Thermal Index (TIC): The Thermal Index for an exposure condition in which the ultrasound beam passes through bone near the beam entrance into the body.

derated: a derated quantity is one which has been measured in water using standard methods and then multiplied by a derating factor. This accounts for attenuation of the ultrasound field by the tissue between the transducer and a particular location in the body along the beam axis. The derating factor is 0.3 dB/cm-MHz in these guidelines.

derated spatial peak time average intensity: the largest value in an ultrasound beam of any derated time averaged intensity.

dwell time: the amount of time that the transducer is actively transmitting ultrasound while staying in any one place during part of an examination.

rarefactional pressure: the amplitude of a negative instantaneous ultrasonic pressure in an ultrasound beam

Soft Tissue Thermal Index (TIS): The Thermal Index for an exposure model in which the ultrasound beam heats primarily soft tissue.

spatial average, pulse average intensity at the face of the transducer: the spatial average, temporal average intensity at the face of the transducer divided by the duty factor, where the duty factor is the product of the pulse duration and the pulse repetition frequency.

spatial average, temporal average intensity at the face of the transducer: the time averaged intensity, averaged over the face of the transducer.

Thermal Index (TI): a quantity related to the potential for **ultrasonic heating**. It is proportional to a calculated or estimated temperature rise for model exposure conditions. The **Thermal Index** is given by the ratio of the ultrasonic power emitted by the transducer to the ultrasonic power required to raise tissue temperature by 1 °C for the model exposure conditions. In the calculation of all Thermal Indices, the average ultrasonic attenuation in the body is assumed to be 0.3 dB/cm-MHz along the beam axis (e.g., the ultrasonic intensity is reduced by 3 dB, a factor of 2, for a 5 MHz beam, 2 cm into the body along the beam axis).

Mechanical Index (MI): a quantity related to the potential for mechanical effects during a diagnostic ultrasound examination. It is given by the ratio of the largest value in the ultrasound beam of any derated rarefactional pressure to the square root of the transducer frequency. The pressure is in Megapascals (MPa) and the frequency is in MHz.

ultrasonic heating: the heating of tissue (including bone) due to the absorption of ultrasound.

ultrasonic power: the total amount of ultrasound energy emitted by the transducer per unit time.

11.2. Acoustic Output

Acoustic output reporting tables are located on eIFU for the following transducer models:

- C5-2H60-A5
- L12-5N40-A4
- L15-7H40-A5
- L18-7H30-A5
- P5-1S15-A6
- LF9-5N60-A3
- LF11-5H60-A3
- MCV9-5N10-A3

11.3. Vigilance system

This equipment is subject to the TELEMED vigilance system (post-marketing vigilance) in case of potential or real hazards for the patient or for the operator which might occur during normal system functioning, in order to be able to remove them with the best efficiency and timing.

Therefore, if a user records any malfunction or deterioration in the characteristics and/or performances of the device, as well as any inadequacy in the labeling or the instructions for use which might lead to potential or real hazards for a patient or for an operator, we kindly request that you **immediately** inform the TELEMED office or local Competent Authority or our official dealer/distributor including sending us the following form (or reporting the same data contained in this form in some other manner) and **do not use** this device. All data relating to the system can be found on its identification label. In this way we will be able to take all adequate, opportune and effective actions.

Post-Marketing Vigilance Form

Го:	Quality Assurance Department UAB "TELEMED"
	Highway Business Centre
	Savanoriu pr. 178A
	Vilnius, LT-03154
	Lithuania
	Phone1: (+370-5) 2106272
	Phone2: (+370-5) 2106273
	Fax: (+370-5) 2306733
	System/device name
	Serial number
	Description of potential hazard

Notes and suggestions _____

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Contact person/ Department					
Address					
Phone	Fax				
Email					
Date	Signature				

11.4. Returned product form

RETURNED PRODUCT №_____

20__.___.

COMPANY			
ADDRESS			
PRODUCT TELEMED OTHER			
SERIAL NUMBER			
REASON FOR RETURN			
INSTRUCTIONS			
REGISTERED BY			
NC REPORT №			
	ELEMED		
WARRANTY		□ NO	

Rows to be filled by sender: COMPANY•ADDRESS•PRODUCT•SERIAL NUMBER•REASON OF RETURN

12. <u>REVISION HISTORY</u>

REVISION	REVISION COMMENTS	ISSUE DATE
1.0	Initial release of the ArtUs EXT-1H/2H User Guide	2018.10.18
1.1	TROUBLESHOOTING additions, some typo changes	2019.07.02
1.2	Changes in chapter 4. Illustrations updated	2020.01.06
1.3 – 1.4	Updated pictures with new case. Updated the list of transducers	2020.04.21
1.5	Added USB connection current consumption	2020.08.26
1.5.1	Added LF series transducers to Disinfection section 8.3. Updated Declaration of Conformity in section 10. Updated transducer list in section 11.2.	2021.09.13
1.5.2	Added information about ArtUs EXT-2H. Changed connection diagram, section 5.1. Updated Declaration of Conformity, section 10	2021.09.14
1.5.3	Multiple corrections regarding safety and compliance with IEC 60601-1	2021.09.23
1.5.4	Added information on approved power supply	2021.10.06
1.5.5	Changed contact details. Added note about elements check procedure	2021.12.06
1.6	Added transducer model to the compatible disinfectants table	2022.04.20